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Christopher Shepard, Dillon C. Yost, and Yosuke Kanai

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# Electronic Excitation Response of DNA to High-energy Proton Radiation in Water

Christopher Shepard<sup>1</sup>, Dillon C. Yost<sup>3</sup>, Yosuke Kanai<sup>1,2\*</sup>

1. Department of Chemistry, University of North Carolina at Chapel Hill; Chapel Hill, NC, 27514, USA.

2. Department of Physics and Astronomy, University of North Carolina at Chapel Hill; Chapel Hill, NC, 27514, USA

3. Department of Materials Science and Engineering, Massachusetts Institute of Technology; Cambridge, MA, 02139, USA.

\*Corresponding author. **Email:** [ykanai@unc.edu](mailto:ykanai@unc.edu)

## Abstract:

The lack of molecular-level understanding for the electronic excitation response of DNA to charged particle radiation, such as high-energy protons, remains a fundamental scientific bottleneck in advancing proton and other ion beam cancer therapies. In particular, the dependence of different types of DNA damage on high-energy protons represents a significant knowledge void. Here we employ first-principles real-time time-dependent density functional theory simulation, using a massively-parallel supercomputer, to unravel the quantum-mechanical details of the energy transfer from high-energy protons to DNA in water. The calculations reveal that protons deposit significantly more energy onto the DNA sugar-phosphate side chains than onto the nucleobases, and greater energy transfer is expected onto the DNA side chains than onto water. As a result of this electronic stopping process, highly energetic holes are generated on the DNA side chains as a source of oxidative damage.

## Introduction

Understanding the radiation-induced response of DNA is pivotal for human health. The electronic excitation induced in DNA by high-energy protons is of great importance to understanding how DNA damage occurs in extreme conditions such as those experienced by astronauts. For instance, as much as 90% of galactic cosmic radiation (GCR) is high-energy protons, and human exposure to GCR is a great concern for space missions, as limited data exists on the bodily effects [2]. The electronic excitation response of DNA to high-energy protons is also the foundation of modern proton beam cancer therapy. Over the past 30 years, proton beam therapy has emerged as a promising alternative to conventional X-rays in radiation oncology [3]. Having a spatially-localized energy deposition profile, with the so-called Bragg peak being its maximum, the ion beam can more precisely target tumor cells, while minimally

affecting surrounding healthy cells [4, 5]. In proton beam therapy, the energy deposition profile needs to be developed for individual patients, and the velocity-dependent energy transfer rate from irradiating protons in water plays a central role [6, 7]. This quantity, often called linear energy transfer or electronic stopping power, is given per unit distance traveled by irradiating protons. The initial kinetic energy of the protons is on the order of a few hundred MeV. As the protons slow down by transferring their momentum, the stopping power increases greatly near the Bragg peak velocity. In addition to having the ideal energy transfer behavior, many studies indicate that proton beams yield complex clustering lesions with strand breaks, including double-strand breaks, as the direct effect on DNA [8]. These strand lesions, particularly with other lesions nearby, are much more likely to lead to cell death [9]. However, how the proton beam induces DNA lesions is not understood at the

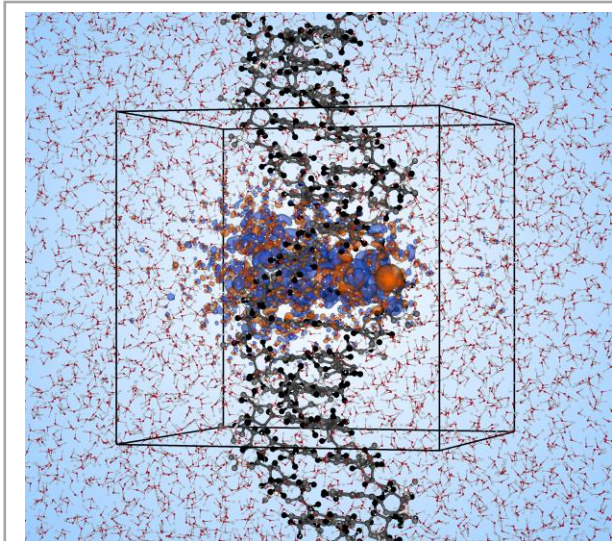


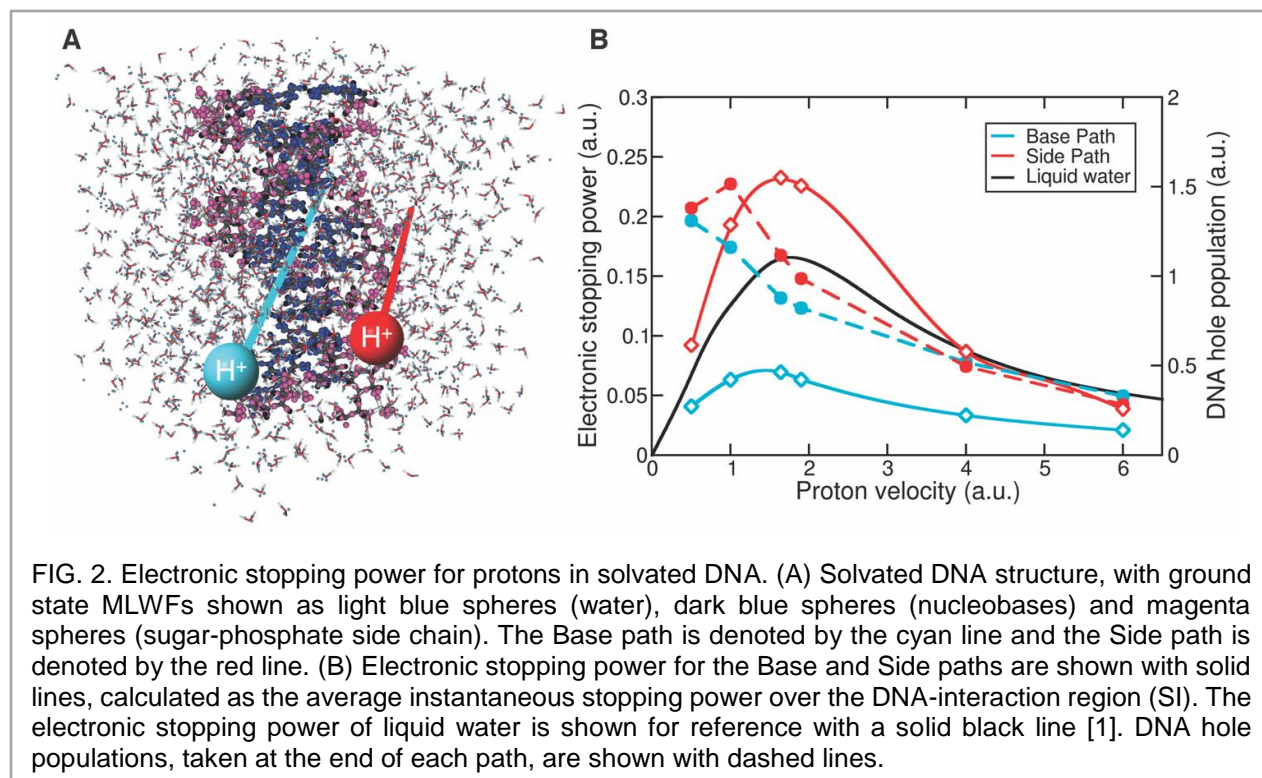
FIG. 1. Simulation cell for solvated DNA. The simulation cell, outlined in black, is shown with periodic boundary conditions for solvated DNA. Blue (orange) isosurfaces represent decreases (increases) in electron density in response to a proton moving through the center of DNA at 0.50 a.u. velocity (6.25 KeV).

molecular level [10], and details of the energy transfer mechanism from irradiating protons to DNA are needed to help fill this crucial knowledge gap [11]. The ultrafast nature of the excitations and the need for a particle accelerator, like a cyclotron, to generate high-energy protons makes experimental investigation difficult [12]. On the theory side, perturbation theories based on the dielectric function are widely used, and the current state-of-the-art approach builds on developing an accurate energy-loss function for dry DNA and liquid water as the target [13-16]. Modern quantum-mechanical simulation offers an alternative approach for investigating such electronic stopping phenomena on the molecular level [17, 18]. Non-equilibrium simulations of electron dynamics have significantly benefitted from recent advances in massively-parallel computers with peta- and exa- floating point operations per second performance [19], and unraveling the quantum-mechanical details at the molecular level has impacted various research areas [20, 21]. In particular, with the development of *time-dependent density functional theory* in its explicit *real-time* propagation form (RT-TDDFT), it

is now possible to investigate the quantum dynamic response of electrons in systems of great chemical complexity, such as DNA in water, as required here for studying electronic stopping. Using large-scale RT-TDDFT simulations [21-23], we show here that high energy protons transfer significantly more energy to the sugar phosphate side chains than the nucleobases of DNA, generating highly energetic holes on the side chains as key source of oxidative damage.

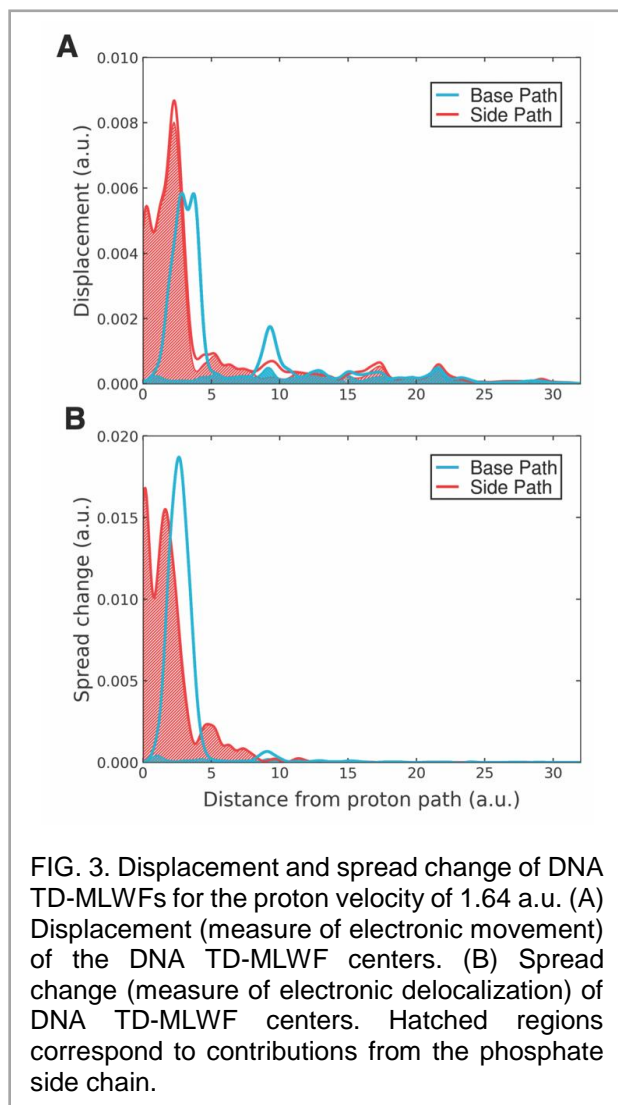
## Results and Discussion

Figure 1 shows B-DNA (i.e. normal right-handed DNA [24]), solvated in water, with the simulation cell outlined by the black box. The DNA strand within the simulation cell comprises one full turn of the double helix. Including the surrounding water molecules, the dynamics of more than 11,500 electrons are explicitly simulated as they respond to an irradiating proton. Additional computational details are discussed in the Computational Method section of the Supplemental Material [25]. In our previous work on dry DNA [26], this first-principles approach was used and compared to the widely-used semi-empirical perturbation theory formalism, based on the dielectric function [13], showing good agreement. We consider two paths for an irradiating proton as shown in Fig. 2A; the Base path directly through the center of the DNA molecule (shown in cyan in Fig. 2A and Fig. S1), and the Side path along the sugar-phosphate side chain (shown in red in Fig. 2A and Fig. S1). Simulations were performed at six different proton kinetic energies (0.5 to 6.0 a.u. velocity, or equivalently 6.25 to 900 keV kinetic energy) for each path, including velocities close to the Bragg peak in dry DNA [26] and liquid water [1]. All atoms, other than the irradiating proton, are fixed in place to study the electronic stopping phenomenon here, and the time scale of each simulation (0.27 to 3.38 fs, depending on proton velocity) is too short for any significant nuclear motion [27]. The energy transfer rate, referred to as electronic stopping power, can be obtained as a function of the proton velocity for each individual path [28]. It is convenient to express the stopping power in terms of the work done on the non-equilibrium system of electrons by a single “projectile” proton, and the total



electronic energy change of the system can be used in practical computation of the stopping power (see Supplemental Material for details [25]) [21]. Comparison of the solvated DNA stopping power curves (Fig. 2B, solid lines) reveals that the stopping power magnitude for the Side path is more than three times larger than that for the Base path at the peak, and at least twice as large at all velocities. This difference increasingly diminishes with higher proton velocities. While the Bragg peak positions for both paths remains similar to that of liquid water [1] (Fig. 2B, black line), the stopping power magnitude for the Side path is 40% larger at the Bragg peak. This is of particular importance as the electronic stopping power for liquid water is generally used for calibrating proton beam in radiation oncology [29]. We also note that at the higher velocities of 4.00 and 6.00 a.u., the stopping power magnitude for the Side path is nearly identical to that of liquid water. Compared to the case of dry DNA [26], the Side path also shows much larger electronic stopping power for solvated DNA (see Fig. S3). Negative charges, specifically lone-pair electrons on phosphate groups on the DNA side chains, were found to be largely responsible for this difference (see Supplemental

Material for details [25]). In order to gain molecular-level insights in this complex system, we employ the time-dependent maximally-localized Wannier function (TD-MLWF) gauge [30, 31]. TD-MLWFs are spatially localized on different chemical moieties, creating a chemically intuitive picture of the DNA-water electronic system. Geometric centers of the TD-MLWFs, commonly referred to as Wannier centers (WCs), are shown in Fig. 2A. The TD-MLWFs can be grouped into different chemical subgroups, and the electronic response of DNA can be separated from that of the solvating water molecules. The response is further studied in terms of DNA chemical moieties, nucleobases and sugar phosphate side chains, by analyzing changes to the spatial spread (Wannier center variance) and Wannier center displacement of individual TD-MLWFs. Figure 3 shows the Wannier center displacements (A) and spread changes (B) for the two paths at the proton velocity of 1.64 a.u. (67.19 keV), close to the Bragg peak. For both paths, greater than 80% of the Wannier center displacements are within 10 a.u. of the proton path, and more than 90% of the spread changes are within 5 a.u. of the proton path; the electronic excitation response is highly localized near the path



of the irradiating proton. In Fig. 3, the hatched areas indicate contributions from the sugar phosphate side chain. The response for the Side path is almost entirely from the phosphate side chain, greater than 87% of the displacements and more than 98% of the spread changes, while the Base path shows minimal contribution from the phosphate side chain, with over 75% of the displacements and more than 90% of the spread change from nucleobases. These key excitation features are also observed at higher and lower velocities (see Figs. S6, S7 in Supplemental Material [25]). Our simulations show that the sugar phosphate side chain molecules absorb much more energy than nucleobases in the proton beam.

Electronic stopping power is often thought to be directly proportional to electronic excitations, or more specifically the number density (i.e. population) of holes (or excited electrons) generated under ionizing radiation [32]. Figure 2B also shows the formation of holes on DNA as a function of the irradiating proton velocity (dashed lines). The DNA hole populations were found to reach a constant value by the end of each simulation trajectory, and charge transfer from DNA to the irradiating proton does not contribute to the hole population (see Supplemental Material for details [25]). While the stopping power is considerably different between the two paths, the hole population is only slightly larger for the Side path. For the 1.00 a.u. proton velocity, where the largest difference in DNA hole population is observed, 1.3 times as many holes are generated for the Side Path relative to the Base Path. However, the stopping power is more than three times greater for the Side Path at the same velocity, relative to the Base Path. Therefore, the differences in electronic stopping power cannot be explained simply by the number density of holes formed on DNA. The stopping power also depends on the energetics of the generated holes. To quantify the energetics, we project the DNA-localized TD-MLWFs onto the energy eigenstates. Figure 4 shows the hole population on DNA as a function of energy for the Base path (A) and the Side path (B). The electronic density of states (DOS) is also shown as a reference (dashed line). A significant number of holes are formed in the deeper lying states for the Side path, and essentially no holes are formed within approximately 2 eV of the highest occupied molecular orbital (HOMO), which is aligned at 0 eV in Fig. 4. The HOMO in DNA largely comprises nucleobase electronic states, and the Base path shows a sharp peak close to HOMO, which is responsible for 10-15% of the holes generated on DNA, depending on the irradiating proton velocity. The deeper-lying DNA-states, at around -20 eV, largely derive from the DNA sugar-phosphate side chains. For the Side path, as much as 8% of the total DNA holes are generated between -20 and -25 eV. At the same time, holes generated in this energy range represent only 2% or less of the total hole



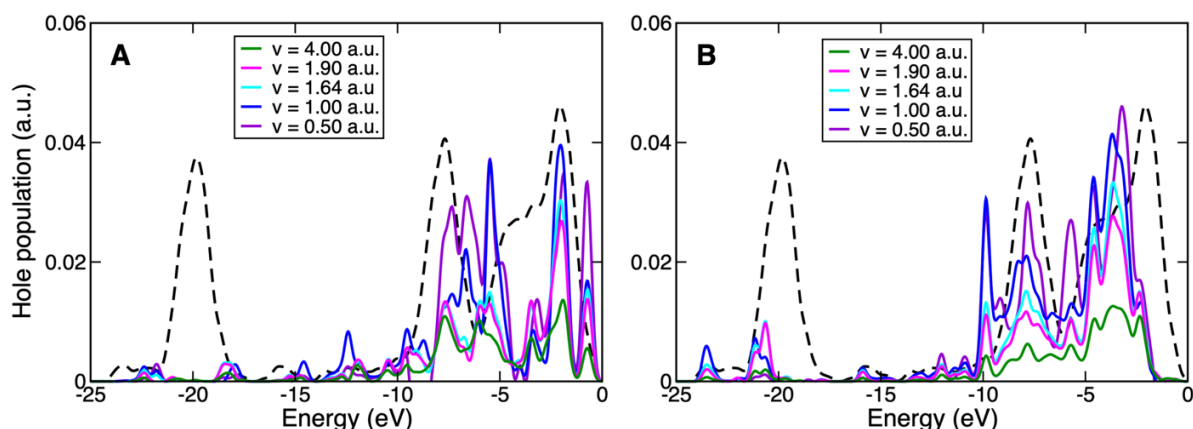


FIG. 4. DNA hole populations as a function of energy for the Base (A) and Side (B) paths. DNA TD-MLWFs are projected onto the eigenstates of the system at equilibrium to calculate the energies at which holes are generated in DNA at the end of simulations. For reference, the density of states is shown with a dashed line. Gaussian broadening of 0.25 eV was used for all hole energy distributions. HOMO is aligned to be at 0 eV. Nearly identical energetics were observed at the end of the DNA-interaction region (see Figs. S10, S11 in Supplemental Material).

population for the Base path, depending on the proton velocity. This characteristic difference in hole energetics is largely responsible for the significant difference in the stopping power for these two paths, and more extensive DNA phosphate side chain damage can be expected than DNA nucleobase damage, under proton irradiation. Additionally, at velocities away from the Bragg peak (e.g. 4.00 and 0.50 a.u., above and below the Bragg peak respectively), the hole generation in the deeper-lying regions (corresponding to the sugar-phosphate side chains) becomes quite small, as seen in Fig. 4. Thus, significant strand damage to DNA can be expected only for proton velocities close to the Bragg peak.

### Conclusion

The electronic excitation response of DNA to high-energy protons in water was investigated. Quantum-mechanical simulations revealed intricate molecular-level details of the energy transfer process from the high-energy protons to DNA in water. With proton irradiation, significantly more energy was deposited onto the sugar-phosphate side chains rather than onto the nucleobases. The enhanced energy transfer to the DNA strands derives from the generation of highly energetic holes on the side chains. These highly energetic holes are a key source of oxidative

damage, and their formation on the side chains is likely the source of DNA strand damage. The first-principles simulation results presented here fill a key knowledge void in understanding detailed mechanisms for extensive DNA strand break lesions observed with a proton beam. In the context of proton beam cancer therapy, the present work will add to the growing knowledge base for building increasingly more sophisticated multi-scale modeling in medical physics [16, 33, 34].

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